



IRCCS Istituto in tecnologie avanzate e modelli assistenziali in oncologia



# Compressione, dose e qualità (clinica) dell'immagine

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CORSO
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# Compression in mammography

Vajuhudeen, Z., Haouimi, A. Compression in mammography. Reference article, Radiopaedia.org. (accessed on 10 Dec 2021) <a href="https://doi.org/10.53347/rID-80054">https://doi.org/10.53347/rID-80054</a>

In mammography, compression of the breast is performed to reduce its thickness. By doing so, the following benefits are achieved:

- improved subject contrast (by reducing scattered radiation)
- >improved density uniformity
- improved visualization of breast tissue near chest wall (by spreading out superimposed anatomy
- >decreased radiation dose
- decreased blurring (by reducing motion artifact)
- Compression is performed by the use of compression paddles, a component of the mammographic unit, which can vary in size and function.

# Q: Compression force... how much it's enough?

In x-ray mammography, it is well known that the flattening of the breast improves image quality and reduces absorbed dose (citare Amended 2014 (Resolution 39)\* ACR—AAPM—SIIM PRACTICE PARAMETER FOR DETERMINANTS OF IMAGE QUALITY IN DIGITAL MAMMOGRAPHY).

In the Euref protocol is stated: "The compression of the breast tissue should be firm but tolerable. There is no optimal value known for the force, but attention should be given to the applied compression and the accuracy of the indication."

# Mean glandular dose

Vajuhudeen, Z., Singh, S. Mean glandular dose. Reference article, Radiopaedia.org. (accessed on 10 Dec 2021) <a href="https://doi.org/10.53347/rID-79640">https://doi.org/10.53347/rID-79640</a>

The **mean glandular dose (MGD)** is an estimate of the average <u>absorbed dose</u> to the glandular tissues of a breast during mammography. It is measured in <u>Gray (Gy)</u>.

The most commonly accepted method of calculating the mean glandular dose is described by *Dance* et al (2000):

$$MGD = K * g * c * s$$

K = entrant surface air kerma

g = conversion factor for 50% glandular breast based on thickness and half-value layer

c = correction factor based on non-standard glandularity/thickness

s = correction factor based on non-molybdenum anode/filter combination

# Q: DOSE... how much it's «ALARA»?

In the Euref protocol Executive summary is stated: "A prerequisite for a successful screening project is that the mammograms contain sufficient diagnostic information to be able to detect breast cancer, using as low a radiation dose as is reasonably achievable (ALARA)."

Table 1.4:	Dose levels for typical breasts simulated with PMMA
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Thickness of PMMA (mm)	Equivalent breast thickness	Maximum average glandular dose to equivalent breasts (mGy)		
	(mm)	Acceptable level	Achievable	
			level	
20	21	≤ 1.0	≤ 0.6	
30	32	≤ 1.5	≤ 1.0	
40	45	≤ 2.0	≤ 1.6	
45	53	≤ 2.5	≤ 2.0	
50	60	≤ 3.0	≤ 2.4	
60	75	≤ 4.5	≤ 3.6	
70	90	≤ 6.5	≤ 5.1	

# **FOMOSYNTHESIS**

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DBT system	Equivalent breast thickness (mm)	Anode/filter	kVp	mAs	AGD 3D	3D vs 2D AGD ratio
Dimensions	21	W/A1	26	30	0.77	1.42
	32	W/A1	28	31	0.91	1.21
	45	W/A1	30	37	1.14	1.18
	53	W/A1	31	46	1.52	1.49
	60	W/A1	33	47	1.80	1.18
	75	W/Al	36	59	2.58	1.41
	90	W/A1	42	55	3.21	1.57
Innovality ST	21	W/Al	27	27.8	0.91	1.75
•	32	W/A1	29	26.4	0.93	1.24
	45	W/A1	31	30.0	1.18	1.20
	53	W/A1	32	36.7	1.53	1.36
	60	W/A1	33	40.8	1.87	1.52
	75	W/A1	36	45.0	2,42	1.28
	90	W/Al	37	56.0	3.05	1.34
Innovality HR	21	W/A1	27	32.9	1.08	2.07
	32	W/A1	29	41.9	1.48	1.98
	45	W/A1	31	58.2	2.28	2.33
	53	W/A1	32	71.5	2.97	2.64
	60	W/A1	33	77.4	3.54	2.88
	75	W/A1	35	83.2	4.24	2.25
	90	W/A1	37	99.0	4.48	1.96
SenoClaire	21	Mo/Mo	26	40.0	0.95	1.66
	32	Rh/Rh	29	33.0	1.03	1.28
	45	Rh/Rh	29	50.0	1.40	1.17
	53	Rh/Rh	29	56.0	1.51	0.91
	60	Rh/Rh	29	75.0	1.91	1.48
	75	Rh/Rh	31	83.0	2.52	1.20
	90	Rh/Rh	31	128.0	3.51	1.43
Pristina	21	Mo/Mo	26	23.1	0.60	0.95
	32	Mo/Mo	26	54.4	1.02	0.99
	45	Rh/Ag	34	28.2	1,22	0.95
	53	Rh/Ag	34	33.7	1.33	0.98
	60	Rh/Ag	34	41.1	1.50	0.98
	75	Rh/Ag	34	60.1	1.91	0.97
	90	Rh/Ag	34	90.7	2.56	0.97

Table 2. Exposure parameters and average glandular doses evaluated for different PMMA thickness for the systems studied in DBT mode.

C.8.31 Breast Projection Image Modules		
<u>Prev</u>	C.8 Modality Specific Modules	<u>Next</u>

#### C.8.31 Breast Projection Image Modules

«1» means MANDATORY

#### C.8.31.1 Enhanced Mammography Image Module

<u>Table C.8.31-1</u> specifies the Attributes that identify and describe general information about the Enhanced Mammography Image Module.

#### Table C 3.31-1. Enhanced Mammography Image Module Attributes

Body Part Thickness	(0018,11A0)	1	The average thickness in mm of the body part examined when compressed, if compression has been applied during exposure.
Compression Force	(0018,11A2)	1	The compression force applied to the body part during exposure, measured in Newtons.
Paddle Description	(0018,11A4)	1	Description of the compression paddle, if compression was applied to the body part during exposure.
Exposure Control Mode	(0018,7060)	1	Type of exposure control Defined Terms: AUTOMATIC MANUAL
Organ Dose	(0040,0316)	1	Organ dose value measured in dGy representing the collective total for all acquired frames.  Note  This may be an estimated value.
Entrance Dose in mGy	(0040,8302)	1	Entrance dose value measured in mGy at the surface of the patient representing the collective total for all acquired frames.  Note  This may be an estimated value based on assumptions about the patient's body size and habitus.
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# Reggio Emilia's provincial breast diagnosis network



At the beginning (2012) 11 GE Senographe Essential units (3 CESM + 3 DBT)

Today 10 GE Senographe Essential units +
1 Pristina
(4 CESM + 11 DBT)

Breast screening program
From 45 to 49 every year - from 50 to 74 every 2 years

Workload activity (2019)

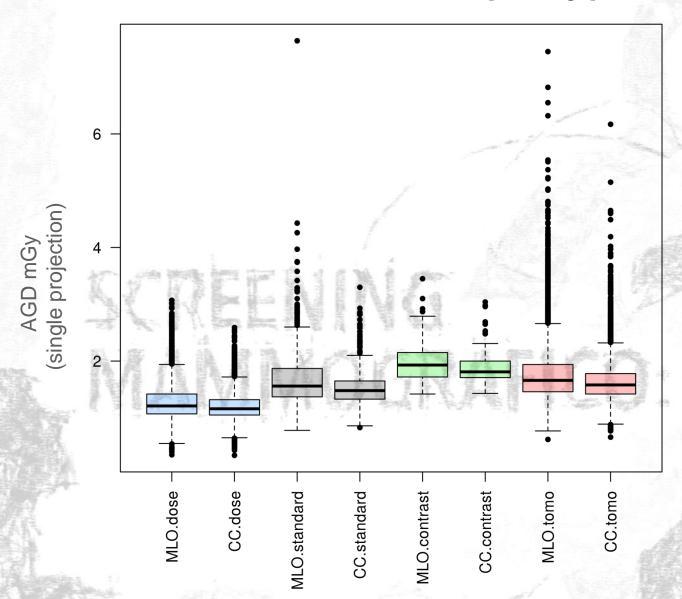
about 49.937 women (+ 19.520 diagnostic exams)

Target population @ 2019 ~ 103.000 women Screening program: adhesion ~79%

Radiographer → each workshift ~ 30 invited women

For 2D MX → three automatic exposure control modes with increasing dose levels are selectable ("DOSE", "STANDARD" and "CONTRAST")

# AGD (mGy) vs AOP\* mode



\* 2D MG offers three automatic exposure control modes with increasing dose levels ("DOSE", "STANDARD" and "CONTRAST"), while DBT uses a single mode ("TOMO").

	AOP>	DBT		2D	
	AUP>	томо	DOSE	STANDARD	CONTRAST
	1st Qu.	1,44	1,06	1,35	1,72
AGD (mGy)	Median	1,61	1,18	1,51	1,85
	3rd Qu.	1,85	1,37	1,77	2,05
	1st Qu.	43	44	43	44
Thickness (mm)	Median	53	53	54	52
	3rd Qu.	61	62	63	59
	1st Qu.	100	100	100	100
Compression (daN)	Median	110	110	110	110
	3rd Qu.	130	130	130	120
	1st Qu.	9	21	24	21
Glandularity (%) (fibrogl/ fat))	Median	20	40	43	39
	3rd Qu.	29	65	67	67
	# projections	15796	14196	1307	293

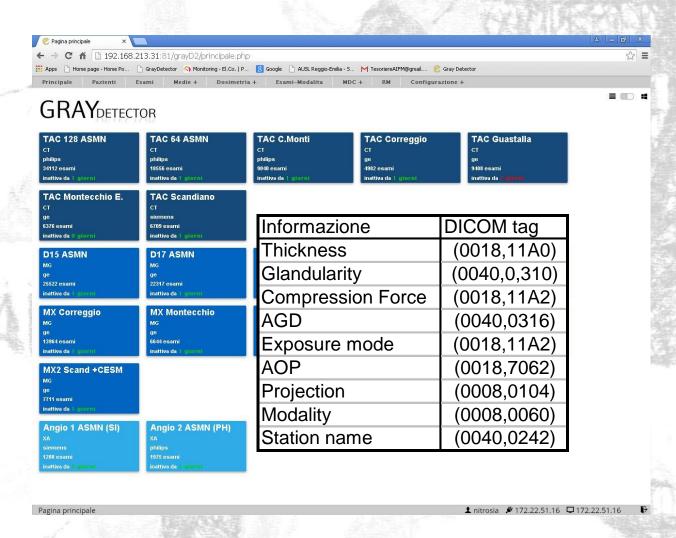
Results reported are referred to 3949 women who performed both 2D (CC-MLO) and DBT (CC+MLO) exams within a clinical trial

In 2014 Reggio Emilia Diagnostic Imaging Department (REDID) adopted a RIS-PACS integrated dose monitoring system called "Gray Detector"\*. It records data from CT, mammography and angiographic examinations.

For mammography
AGD, compression,
thickness, glandularity,
automatic exposure control
(AOP mode),
are collected for
EACH PROJECTION\*

@ Dec 10st 2021 more than 1,400,000 2D MX\* 180,000 DBT\*

Patient dose management solution directly integrated in the RIS: "Gray Detector" software. Nitrosi A et al J Digit Imaging. 2014 Dec;27(6):786-93



# Why AGD vary so much?



AGD variation ~ 60%

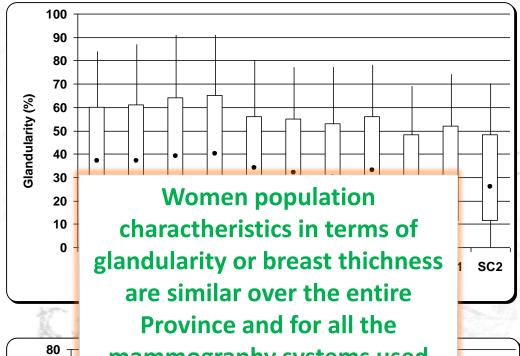
# Mammograhy unit

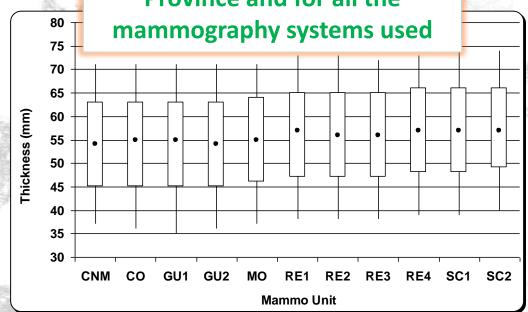
Physical charaterization of 11 mammo Units Variation < 4 %

	Output	HVL
	Output	28 kV
Ι.	μGy/mAs (1m)	Mo/Mo
CM	49,69	0,385
CO	49,37	0,384
GU1	51,22	0,381
GU2	51,01	0,381
MO	50,51	0,386
RE1	50,34	0,390
RE2	50,45	0,385
RE3	51,59	0,382
RE4	51,48	0,382
SC1	49,59	0,384
SC2	51,09	0,383

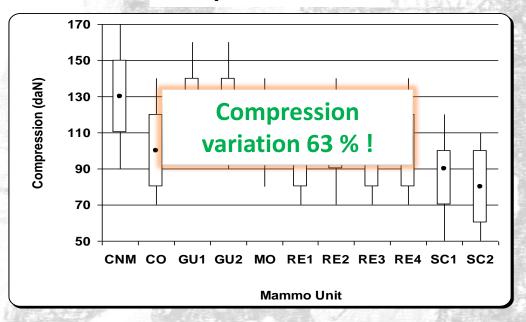
Variation < 2 %

# **Glandularity**



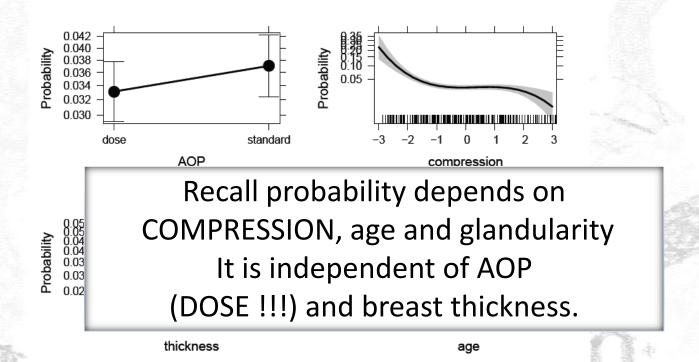


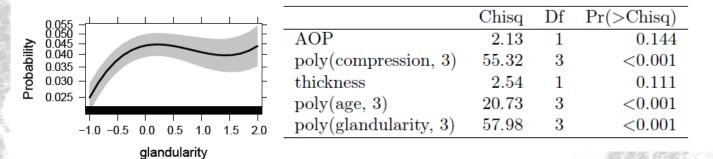
# **Compression force**

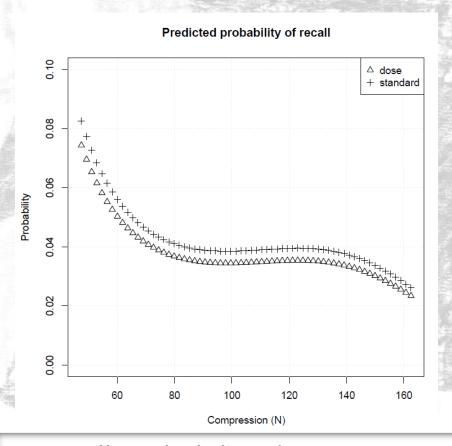


AOP	Negative	Recall	Recall Rate
Dose	11,947	447	3.61%
Standard	8,714	373	4.10%
Contrast	263	8	2.95%

# Recall probability linear mixed effects model analysis







Recall probability descrease in function of compression and became stable over 90/100 N

# Q: Compression force... how much it's enough?

In x-ray mammography, it is well known that the flattening of the breast improves image quality and reduces absorbed dose (citare Amended 2014 (Resolution 39)\* ACR—AAPM—SIIM PRACTICE PARAMETER FOR DETERMINANTS OF IMAGE QUALITY IN DIGITAL MAMMOGRAPHY).

In the Euref protocol is stated: "The compression of the breast tissue should be firm but tolerable. There is no optimal value known for the force, but attention should be given to the applied compression and the accuracy of the indication."

→A: Since no optimal value is known our observation on recall rate dependence from compression force was used: the application of a compression force of at least 100N was suggested to the each radiographer.

# Please adopt a standard!

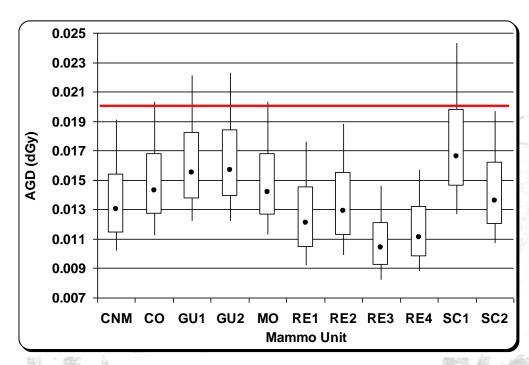
- → AOP selection = DOSE
- → Compression Force ~ 100 N

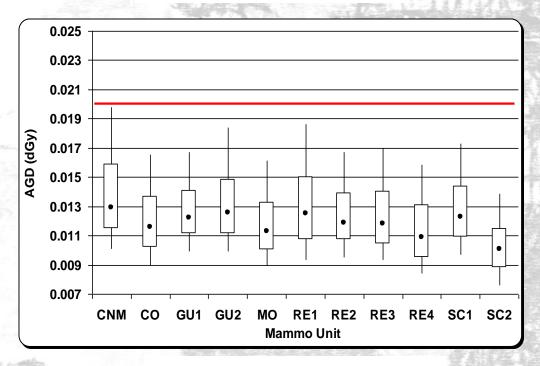
Results compare periods before and after this standardization (Jan-May Vs Jun-Dec 2014)

	Jan-May 2014	Jun-Dec 2014*
# Women	14,108	13,987

**PRE-Standardization** 

## **POST-Standardization**





Variation: 60%

Mean AGD: 1.4 mGy

- 14%

Variation: 28%

Mean AGD: 1.2 mGy

Standardization... It's not enough !!!

(Clinical) Image Quality Control is needed!

# Standardization compression force and AOP selection → lower dose and variability



# **Clinical control**

Image quality... in a BSP ~

- → higher performance (cancer detection rate DR)
  - → more stable performance (recall rate RR)

= 1° optimization step

# Standardization + Clinical control = 1° optimization step

Standardization

Clinical control

Jan-May 20	
14.108	
,	13,987
1 12	1 07
1.38 to 1.22	mGy
1.64	1.44
46.3	<b>45</b> 0
s 1-2 mm lov	wer
64.5	63.0
17 Г	10.2
ity ~ 2 % hig	her
59.3	62.3
00	100
gher & more	e uniform
120	123
	1.38 to 1.22  1.64  1.64  1.63  5 1-2 mm lov  64.5  17.5  ity ~ 2 % high  59.3  gher & more

James - 46 decre ill aller			
	Jan-May 2014	Jun-Dec 2014*	
# Women	14,108	13,987	
# Pocalic	ЛОЛ	611	
Detection rate increse of about 15 %!!!			
# True positive	63	71	
Detection Rate DR ‰	4.47	5.08	

# Linear mixed effects model analysis

# **Discrepancy between 1st - 2nd reader**

	OR	2.5%	97.5%
2nd Period	1.094	0.965	1.242
AOP STD	0.834	0.678	1.025
AOP CNT	0.642	0.375	1.048
Thickness	0.988	0.976	1.001
Compression Force	0.999	0.999	1.000
AGD	1.595	1.127	2.226
Glandularity	1.020	1.012	1.029
I(Glandularity^2)	1.000	1.000	1.000
Age	0.757	0.684	0.839
I(age^2)	1.002	1.001	1.003

Fixed effects

- AOP dose
- first period

AGD seem to be significant ... further analysis demonstrate that, for both periods, the reader concordance were higher (3.14 % Vs 2.59 %) for lower dose level

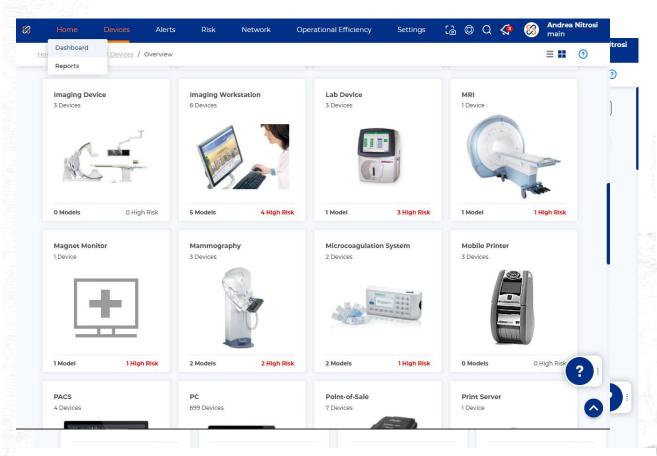
# Recalls

LAIVIINT	OR	2.5%	97.5%
2nd Period	1.274	1.118	1.454
AOP STD	0.822	0.693	0.972
AOP CNT	1.035	0.658	1.546
Thickness	0.978	0.960	0.997
I(Thickness^2)	1.000	1.000	1.000
Compression Force	0.999	0.999	1.000
Glandularity	1.027	1.019	1.036
I(Glandularity^2)	1.000	1.000	1.000
Age	0.733	0.660	0.814
I(age^2)	1.003	1.002	1.003

Fixed effects

- AOP dose
- first period

Only "Period" seem to be significant.

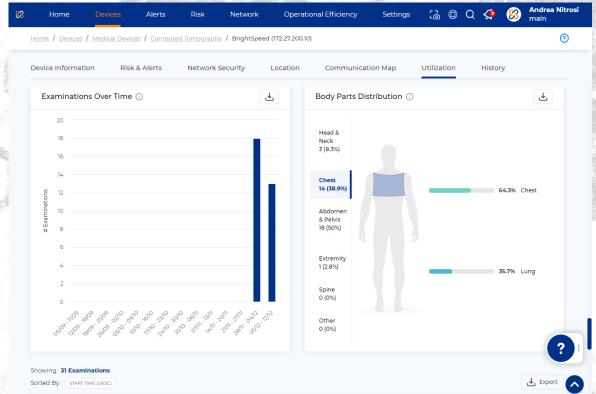


Security Platform Agent can discovers and profiles every connected device, analyzes their risks, and automates responses to keep it safe and operating efficiently.

For some of that for medical device profiles, contextual anomaly detection (e.g. FDA warning), and risk identification with a unique approach are available, too!

Is it necessary to have a dose monitoring system to do this type of analysis?

Not anymore ... in principle it is NOT necessary to configure nodes and connections on modality / RIS / PACS / RDS but simply to "listen" the network!



### Journal of Medical Radiation Sciences



**REVIEW ARTICLE** 

# Mammographic compression practices of force- and pressure-standardisation protocol: A scoping review

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#### Keywords

breast, mammographer, mammography, review, screening

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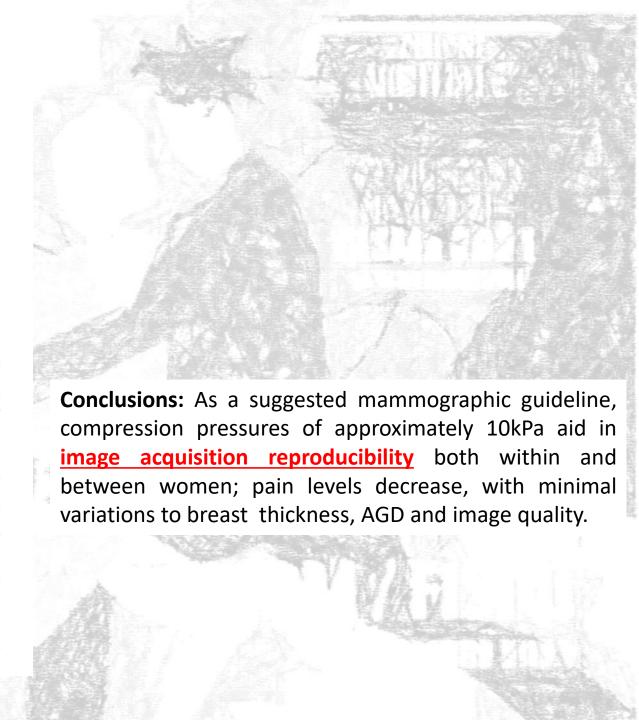
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J Med Radiat Sci 67 (2020) 233-242

doi: 10.1002/jmrs.400

#### Abstract

Introduction: As an efficient, effective and moderately inexpensive modality, mammography has been implemented as a cancer screening tool and in diagnostic management. However, appropriate breast compression is necessary for optimal outcomes. Current key measures of compression force are subjective and variable, giving rise to the concept of a 'personalised' pressurestandardisation protocol. Methods: A scoping review of the literature was performed using the Arksey and O'Malley framework to explore the existing force- and pressure-standardisation protocols in clinical application. A comprehensive search strategy and standardised study selection and evaluation were completed. This synthesis of existing knowledge can lead to the implementation of mechanically standardised mammographic compression pressure as a feasible tailored approach to clinical practice. Four databases (PubMed, MEDLINE, Embase and Scopus) were searched from the databases' inception to 13 December 2019 for relevant information, and eighteen articles were selected for analysis. Results: In addition to current protocol comparison, emerging key concepts include the reasoning behind standardisation, the benefits of improved diagnostic outcomes/decreased pain with negligible change in image quality and average glandular dose (AGD), and the recommendation of a 10kPa (approximate) pressure-standardisation protocol. Research to date is largely based abroad (Netherlands), with a strong focus on screening practices. Consequently, several gaps in the current literature were identified as potential directions for future investigation. Conclusions: As a suggested mammographic guideline, compression pressures of approximately 10kPa aid in image acquisition reproducibility both within and between women; pain levels decrease, with minimal variations to breast thickness, AGD and image quality.



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# Take it home:

Compression force → To be firm but tolerable

(~100 N for Reggio could be ok)

DOSE > «ALARA»

(~AOP DOSE for Reggio could be ok)

Image quality in a BSP → recall rate RR ? detection rate DR ?

**Dose monitoring systems** (BUT NON ONLY) could allow to standardize and optimize image acquisition setups

Optimization needs continuos monitoring of clinical results over iterative application of standardization process  $\rightarrow$  «Plan Do Check Act»

# Thanks for your attention!

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